RESEARCH ARTICLE

REVISED Reliability and reproducibility of spectral and time domain optical coherence tomography images before and after correction for patients with age-related macular degeneration [version 2; peer review: 2 approved, 1 approved with reservations]

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Abstract

Purpose: To evaluate the reproducibility and reliability of optical coherence tomography scans obtained using the time domain (TD-OCT) Stratus™ OCT, and the Spectral Domain (SD-OCT) Spectralis™ and Cirrus™ OCT devices before and after manual correction in eyes with either Neovascular (NV-AMD) or Non-Neovascular (NNV-AMD) age-related macular degeneration.

Design: Prospective observational study.

Methods:

Setting: University-based retina practice.

Patients: Thirty-six patients (50 eyes) with NV-AMD or NNV-AMD.

Procedure: OCT scans were taken simultaneously using one TD-OCT and two SD-OCT devices.

Main Outcome Measures: Macular thickness measurements were assessed before and after correction of the algorithm by constructing Bland-Altman plots for agreement and calculating intraclass correlation coefficients (ICCs) and coefficients of repeatability (COR) to evaluate intraclass repeatability.

Results: Spectralis had the highest number of images needing manual correction. All machines had high ICCs, with Spectralis having the highest. Also, Bland-Altman plots indicated that there was low agreement between Cirrus™ and Stratus™, Spectralis™ and Stratus™, while there was good agreement between the Cirrus™ and Spectralis™. The CORs were lowest for Spectralis™ and similar and higher for Cirrus™ and Stratus™. Agreement, CORs, and ICCs generally improved after manual correction, but only minimally.

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Any reports and responses or comments on the article can be found at the end of the article.

Conclusion: Agreement is low between devices, except between both SD-OCT machines. Manual correction tends to improve results.

Keywords

age related macular degeneration , neovascularization , optical coherence tomography , spectral domain , time domain

This article is included in the **Eye Health** gateway.

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REVISED Amendments from Version 1

The following changes were made to this version:

1. The author list and affiliations were updated.
2. Author contributions section was updated accordingly.
3. The statement "To date, no other study has examined the effects of manual correction of the thickness algorithm in SD-OCT and TD-OCT machines in eyes with AMD" was removed from the introduction section.
4. Details of the grading process and segmentation correction procedures were updated in the methods section under the subheading "Error determination, manual correction, and exclusion of scans".
5. The following statement was added to the statistical analysis section: "No formal sample size calculation was performed before performing the study".
6. A study highlighting the reproducibility of segmentation error correction in age-related macular degeneration using Stratus and Cirrus OCT by Krebs *et al.* was discussed in the discussion section.
7. Differences in the mean thickness values of the central and peripheral subfields before and after correction in scans taken using Spectralis were discussed.
8. Additional study limitations and possible sources of bias were identified in the discussion section.

See referee reports

Introduction

Optical Coherence Tomography (OCT) is a non-invasive imaging modality that allows acquisition of cross-sectional images of the retina. OCT is useful in monitoring and evaluating retinal thickness in many retinal disorders. One example is Age-related Macular Degeneration (AMD), a progressive, blinding disease that is mostly non-neovascular (NNV-AMD) but can be associated with choroidal neovascularization (NV-AMD). Currently, OCT is also being employed as an outcome measure in many multicenter clinical trials of AMD with Time Domain OCT (TD-OCT) device being the most common^{1,2}.

As this technology is increasingly being utilized by many ophthalmologists to evaluate and monitor patients and guide treatment decisions², it is important to understand the reliability and accuracy of thickness measurements obtained with various devices currently available. Recently, studies have shown that in patients with AMD, there is a high frequency of errors in automated retinal thickness measurements due to incorrect segmentation of the retina in the TD-OCT machine specifically in NV-AMD^{2,3}. Using an Spectral Domain OCT (SD-OCT) device Menke *et al.* found that NNV-AMD had fewer errors than NV-AMD, mostly due to the pathology of the disease resulting in retinal pigment epithelial (RPE) layer changes⁴.

Manual correction of the algorithm is an option in newer generations of the review software and as more OCT devices are coming to the market, it is important to understand the clinical importance of manual correction of OCT algorithms and the agreement of thickness measurements from different machines before and after

correction. In our study, we evaluated the intra-session repeatability and agreement in retinal thickness measurements for patients with NV-AMD and NNV-AMD before and after manual correction using three different OCT devices: Stratus™ TD-OCT and two SD-OCTs, Spectralis™ and Cirrus™.

Methods

Institutional Review Board (IRB)/Ethics Committee approval was obtained and HIPAA guidelines were followed for the study. Informed consent was obtained from study subjects.

Patients and scanning

Patients with confirmed diagnosis of AMD were enrolled in the study. Two senior retina specialists (QDN and DVD) made the diagnosis of AMD. Patients under treatment with intravitreal injections of anti-vascular endothelial growth factor (VEGF) agents were also allowed to participate in the study.

Patients were scanned twice by certified OCT operators on a TD-OCT device (Stratus™ OCT) and two SD-OCT devices (Spectralis™, and Cirrus™ OCT) machines in random order and with 5–10 minutes between each device. The same operator performed all the scans on any given patient. Scans on a single device were performed consecutively and 5 minutes apart from each other.

Optical Coherence Tomography

One TD-OCT machine, Stratus™ (software version 4), and two SD-OCT machines, Spectralis™ (software version 5.0 I and Cirrus™ (software version 5.0.0.326) were used. Stratus™ is a TD-OCT machine that uses a super luminescent diode with a wavelength of 820 nm. It provides an axial resolution of 10µm and image acquisition speed of 400 A-scans/second. Using the Stratus™, two fast macular thickness maps (FMTM) were acquired from each eye. The FMTM is created through acquiring six radial B-scans, each consisting of 512 A-scans, and at an angle of 30° from each other with the point of intersection centered on the fovea.

Spectralis™ uses a super luminescent diode with a wavelength of 870 nm. It provides axial resolution of 4µm and image acquisition speeds of up to 40,000 A-scans per second. Two volume scans were acquired from each eye using a raster scan of 19 lines covering 20×15° of the fundus. Using the TruTrack™ functionality of the Spectralis™ OCT, each line was averaged 15 times or more. Cirrus™ HD-OCT also uses a super luminescent diode with a wavelength of 840 nm. It provides images with an axial resolution of 5µm and acquisition speeds of 27,000 A-scans per second. We acquired two 512×128 macular cube scans (128 B-scans and 512 A-scans, covering a retinal area of 6.0×6.0 mm) from each eye.

Error determination, manual correction, and exclusion of scans

Scans from each of the three devices were reviewed at the Ocular Imaging Research and Reading Center at the Stanley M. Truhlsen Eye Institute by two independent graders. Segmentation errors due to incorrect identification of inner and outer retinal boundaries by automated algorithms in the Spectralis™ and Cirrus™ devices were identified and manually corrected by these graders. Stratus™ images could not be corrected due to the lack of editing capabilities in the operating system provided with the machine at the time

of conducting the study. Only 5 patients required corrections and were excluded from the analysis. The proprietary software identifies retinal boundaries for measurement of retinal thickness that are specific to each device. Meanwhile each device identifies the inner limiting membrane (ILM) as the inner boundary of retina, identification of the outer boundary is different for each device. Stratus™ identifies the junction between the inner and outer segments of photoreceptors (IS/OS) as the outer boundary, Spectralis™ identifies the posterior border of the retinal pigment epithelium (RPE), and Cirrus™ identifies the inner border of the RPE as the outer retinal boundary.

Whenever the foveal center could be identified, grids were repositioned for scans with off-center positioning of the ETDRS grid. However, in some cases, morphological changes associated with the advanced disease made identification of the foveal center unreliable. Adjustment of grid position was not possible for Stratus™ OCT. Scans were excluded from analysis only if identification of retinal layers and determination of the retinal thickness was not possible. OCT scans from which extraction of thickness data for the central 1mm sub-field was not reliable, due to missing data in the image or the scan being out of range, were also excluded from analysis.

The retinal thickness measurements of the nine standard ETDRS subfields (Appendix A illustrates the nine-subfield abbreviations) were recorded from each device before and after correcting the errors in the scans algorithm.

Statistical analysis

No formal sample size calculation was performed before the conduct of the study. Bland-Altman plots were constructed to determine agreement between devices; both 95% confidence intervals and limits of agreements were calculated. Reproducibility of measurements was determined by calculating the coefficients of repeatability (COR) for each machine. Intraclass correlation coefficients (ICCs) were used to determine the reproducibility for each

device. Statistical significance of difference in thickness before and after correction of images across devices was determined via student's t-test with $\alpha = 0.05$ with Bonferroni correction for multiple comparisons. STATA version 10 and Microsoft Excel 2007 were used for data management and analysis. The statistical analysis was performed before and after any manual corrections were made to the algorithm errors described above.

Results

Fifty eyes from 36 patients were included in the study; 29 eyes had NV-AMD and 21 eyes had NNV-AMD. The mean age of the study subjects was 76.6 years.

Exclusion and corrections

Stratus™

Scans from four eyes could not be recovered from the database and scans from three eyes had algorithm errors with incorrect identification of retinal boundaries and were excluded from analysis. Scans were not corrected for off-center positioning of the scan as moving the ETDRS grid was not possible with the available software version.

Cirrus™

Scans in six eyes scanned first and eight eyes scanned second were corrected either for off-center fixation of the eye or for incorrect automated identification of retinal boundaries. The thickness measurements before and after correction were not statistically significant ($P < .05$) for any of the subfields and also when stratified by diagnosis.

Spectralis™

Thirty-three scans among the first set and 32 among the second set were corrected. The inner inferior subfield for NV-AMD was the only subfield that was statistically significant before and after correction. Figure 1 plots the frequency of the differences before and after correction for the central subfield for all scans. 77% of the differences were less than 48µm and 50% were less than 10µm.

Figure 1. Frequency of the relative differences of the central 1mm subfield of Spectralis™ images before and after correction.

OCT characteristics

The mean ($\pm$ SD) of the macular thickness of all of the subfields, including the central 1mm subfield (FTH) for Stratus™, Cirrus™, and Spectralis™ before and after manual correction of scans, stratified by diagnosis of NV-AMD and NNV-AMD, is shown in Table 1. For NV-AMD, the FTH values for central 1mm were 375 μ m ($\pm$ 129 μ m), 253 μ m ($\pm$ 74 μ m), 312 μ m ($\pm$ 110 μ m) for Spectralis™, Stratus™, and Cirrus™ respectively. After correction, the values were 335 μ m ($\pm$ 106 μ m) for Spectralis™ and 318 μ m ($\pm$ 110 μ m) for Cirrus™. On the other hand, the FTH values for NNV-AMD in the central 1mm before correction were 298 μ m (87 μ m), 193 μ m ($\pm$ 32 μ m), and 229 μ m ($\pm$ 30 μ m) for Spectralis™, Stratus™, and Cirrus™ respectively. Spectralis™ was the only device to have a different FTH value of 248 μ m ($\pm$ 56 μ m) after correction. Overall, Spectralis™ had the highest retinal thickness values (range: 280 to 372 μ m), depending on the subfield. The retinal thickness measurements obtained via the Cirrus™ were slightly less (range: 230 to 320 μ m), while Stratus™ had the lowest values, ranging from 190 to 270 μ m. There were no significant ($p < .05$) differences between the mean FTH of the first and second scans for each of the three devices.

The central subfield ICC values for all three machines were very high at 99.6%, 97.2% and 96.4% before correction for Spectralis™, Stratus™, and Cirrus™ respectively, and 99.4%, and 97.4% after correction for Spectralis™ and Cirrus™. The ICC values were greater than 95% for all subfields and both diagnoses except the outer inferior field for NNV-AMD for Spectralis™. Stratus™ values ranged from 78.9% to 99.2% for NV-AMD and 94.7% to 99% for NNV-AMD, before and after correction, respectively. Cirrus™ values ranged from 88.5% to 99.9% and 99.1% to 99.8% for NV-AMD before and after correction, respectively. The values for NNV-AMD for Cirrus™ ranged from 99.3% to 99.9% and 71.4% to 99.7% before and after correction, respectively. Table 2 shows the ICC values between images for all three machines before and after correction, both combined and stratified by diagnosis. It should be noted that all of the machines had ICC values $>90\%$ for the central subfield while the Spectralis™ had no subfields less than 99% after correction. In the central subfield, Spectralis™ had a COR of 20 μ m NV-AMD which increased to 23 μ m; both Cirrus™ and Stratus™ had relatively larger CORs of 64 μ m (reduced to 49 μ m after correction) and 35 μ m, respectively. For NNV-AMD, the COR for the central subfield was 15 μ m for both Cirrus™ and Spectralis™, and was 24 μ m for Stratus™. After correction, the value decreased for Spectralis™ to 12 μ m and increased to 36 μ m for Cirrus™. The COR of all subfields for each device before and after correction of algorithms and stratification by disease are given in Table 3.

Overall Spectralis™ had the lowest COR, with values ranging from 5–30 μ m. Cirrus™ and Stratus™ had similar values ranging from 5–70 μ m, even after correction. The COR for Cirrus™ increased by 15–40 μ m after correction for NNV-AMD. Also, Cirrus™ COR values were 10–30 μ m higher than Stratus™ values for both NV-AMD and NNV-AMD. Agreement between machines was poor, except between Spectralis™ and Cirrus™ after correction. Table 4–Table 5 show 95% confidence intervals and limits of agreement of the Bland-Altman plots between devices before and after manual correction.

Figure 2a–f show Bland-Altman plots with 95% confidence intervals for the FTH comparison of the machines before and after correction. Before correction, the mean difference between the machines was 32 μ m for Spectralis™ vs. Cirrus™, 52 μ m for Cirrus™ vs. Stratus™, and 84 μ m for Spectralis™ vs. Stratus™. Manual correction reduced the differences, with it being 15 μ m for Spectralis™ vs. Cirrus™, 51 μ m for Cirrus™ vs. Stratus™, and 67 μ m for Spectralis™ vs. Stratus™. When stratified by diagnoses, the values were 34 μ m and 29 μ m for Spectralis™ vs. Cirrus™, 53 μ m and 47 μ m for Cirrus™ vs. Stratus™, and 88 μ m and 79 μ m for Spectralis™ vs. Stratus™ for NV-AMD and NNV-AMD before correction, respectively. After manual correction, the values reduced to 17 μ m and 14 μ m Spectralis™ vs. Cirrus™ and 70 μ m and 61 μ m Spectralis™ vs. Stratus™ for NV-AMD and NNV-AMD, respectively. The confidence interval widths, on average, were 5–10 μ m smaller than between an SD-OCT and TD-OCT machine. The average interval width decreased between 5–10 μ m after correction for any disease and comparison, except for the Cirrus™ vs. Stratus™ comparison.

Discussion

The advent of OCT has revolutionized the way patients with retinal disorders are evaluated and monitored. However, like every new device, the current devices employing time- or spectral domain technology have certain limitations. One such common and clinically relevant issue is the presence of a random error in the identification of the inner and outer boundaries of the retina by the algorithm. With respect to AMD, studies have shown that in lesions such as fibrotic scars, choroidal neovascularization disrupting the RPE, and subretinal fluid the automated segmentation algorithms would produce errors because the software would not correctly delineate the outer retinal boundary^{3,5}. In our study, we found that 66% of the Spectralis™, 14% of the Cirrus™ and 6.5% of the Stratus™ scans had algorithm errors. Giani *et al.* reported similar results; for Cirrus™, they reported 25% and 16% algorithm error rates for NNV-AMD and NV-AMD, respectively. However, for Spectralis™, they reported 16.67% and 57.6% algorithm error rates and 8.33% and 62.5% rates for Stratus™ for NNV-AMD and NV-AMD, respectively⁵. Other studies have reported Stratus™ outer boundary algorithm errors of approximately 43% for both forms of AMD and 60% for NV-AMD^{3,6}.

Reasons for differences in our error rates compared to previous include a lack of standard definition of an algorithm error. Rather than having an exact definition of an algorithm error, which may not be clinically significant⁵, in our study, the decision was made by two masked observers who determined if the correction would be important. In addition, even though Spectralis™ segments the outer border of the RPE, a study by Jaffe *et al.* reported that it may also be including the Bruch's membrane in its calculation, thus including sub-RPE pathology such as drusen when segmenting the outer border of the retina⁷. These differences may be due to the fact that our study was prospective and while acquiring scans, the operators tried their best to ensure no errors occurred during scan acquisition. Lastly, we did not exclude scans if the signal strength was low or if the machine gave a low analysis confidence message, as other studies have done^{8–10}.

Table 1. A comparison of thickness measurements between two machines demonstrated that most values were significantly different ($p < .05$). Spectralis™ vs. Cirrus™ before correction: for NV-AMD, T1, S1, and I2, and for NNV-AMD, C1, T1, N1, and I2. Spectralis™ vs. Cirrus™ after correction: for NV-AMD every field except S2, and I2 were not significant, and for NNV-AMD, the inner subfields were not significant. Spectralis™ vs. Stratus™ after correction: for NV-AMD, C1.

Subfield	Mean $\pm$ standard deviation (μm)											
	All eyes						NV-AMD					
	Spectralis™			Cirrus™			Spectralis™			Stratus™		
	Before	After	Before	After	Before	After	Before	After	Before	After	Before	After
C1	343 $\pm$ 119	301 $\pm$ 98	229 $\pm$ 67	277 $\pm$ 94	281 $\pm$ 96	375 $\pm$ 129	335 $\pm$ 106	253 $\pm$ 74	312 $\pm$ 110	318 $\pm$ 110	298 $\pm$ 87	248 $\pm$ 56
N1	348 $\pm$ 74	329 $\pm$ 70	267 $\pm$ 50	317 $\pm$ 57	319 $\pm$ 56	370 $\pm$ 81	351 $\pm$ 74	285 $\pm$ 54	336 $\pm$ 61	339 $\pm$ 61	319 $\pm$ 51	297 $\pm$ 51
S1	346 $\pm$ 74	327 $\pm$ 66	260 $\pm$ 40	317 $\pm$ 71	316 $\pm$ 70	372 $\pm$ 84	349 $\pm$ 71	277 $\pm$ 40	342 $\pm$ 80	339 $\pm$ 80	312 $\pm$ 41	295 $\pm$ 44
T1	345 $\pm$ 74	321 $\pm$ 59	250 $\pm$ 46	305 $\pm$ 65	305 $\pm$ 65	366 $\pm$ 83	337 $\pm$ 56	265 $\pm$ 51	325 $\pm$ 75	324 $\pm$ 75	318 $\pm$ 50	297 $\pm$ 57
I1	347 $\pm$ 72	325 $\pm$ 70	256 $\pm$ 59	314 $\pm$ 66	314 $\pm$ 65	362 $\pm$ 78	340 $\pm$ 75	273 $\pm$ 63	329 $\pm$ 75	330 $\pm$ 74	327 $\pm$ 58	302 $\pm$ 58
N2	307 $\pm$ 42	302 $\pm$ 44	250 $\pm$ 49	293 $\pm$ 46	292 $\pm$ 46	317 $\pm$ 49	312 $\pm$ 49	259 $\pm$ 60	302 $\pm$ 56	300 $\pm$ 58	293 $\pm$ 22	288 $\pm$ 31
S2	297 $\pm$ 42	292 $\pm$ 42	223 $\pm$ 28	279 $\pm$ 46	278 $\pm$ 45	310 $\pm$ 47	303 $\pm$ 48	226 $\pm$ 34	291 $\pm$ 54	289 $\pm$ 55	282 $\pm$ 27	278 $\pm$ 28
T2	284 $\pm$ 49	278 $\pm$ 46	220 $\pm$ 45	270 $\pm$ 66	269 $\pm$ 66	292 $\pm$ 54	286 $\pm$ 52	231 $\pm$ 53	283 $\pm$ 81	282 $\pm$ 82	273 $\pm$ 39	266 $\pm$ 36
I2	292 $\pm$ 61	286 $\pm$ 63	233 $\pm$ 55	272 $\pm$ 42	270 $\pm$ 42	303 $\pm$ 75	298 $\pm$ 76	245 $\pm$ 64	278 $\pm$ 46	276 $\pm$ 46	276 $\pm$ 25	268 $\pm$ 28

Table 2. Intraclass correlation coefficient percentages before and after correction.

Subfield	ICC values (%)											
	(All eyes)						NV-AMD					
	Spectralis™			Cirrus™			Spectralis™			Stratus™		
	Before	After	Before	After	Before	After	Before	After	Before	After	Before	After
C1	99.6	99.4	97.2	96.4	97.4	97.4	99.8	99.6	99.6	98.5	98.5	98.4
N1	99	99.5	87.6*	85.6*	84.7*	84.7*	99.4	99.7	99.7	91.9*	91.9*	99.9
S1	99.3	99.5	82.8*	93.8	90.7*	90.7*	99.6	99.7	99.7	86*	86*	98.7
T1	98.2	99	96	95.6	90.4*	90.4*	98.9	99.2	99.2	97.4	97.4	99.3
I1	98.9	99	95.9	95.1	91.2*	91.2*	99.4	99.7	99.7	98.3	98.3	99.4
N2	99.1	99.6	98.4	96.6	96	96	99.7	99.8	99.8	99.2	99.2	99.8
S2	99.6	99.5	71.2*	82*	90.5*	90.5*	99.8	99.6	99.6	88.5*	88.5*	99.5
T2	99.2	99.4	92.7	98.1	98.4	98.4	99.6	99.6	99.6	95.8	95.8	99.5
I2	98.3	99	94.9	95.8	95.6	95.6	99.8	99.4	99.4	97	97	99.4

Table 3. Coefficient of the repeatability values before and after correction.

Coefficient of repeatability (μm)															
Subfield	All eyes					NV-AMD					NNV-AMD				
	Spectralis™		Stratus™	Cirrus™		Spectralis™		Stratus™	Cirrus™		Spectralis™		Stratus™	Cirrus™	
	Before	After	Before	Before	After	Before	After	Before	Before	After	Before	After	Before	Before	After
C1	18	20	31	50	44	20	23	35	64	49	15	12	24	15	36
N1	26	15	26	39	62	23	15	58	74	69	13	8	26	14	46
S1	16	12	49	49	58	20	13	62	63	64	10	10	18	15	48
T1	20	13	48	57	60	32	18	32	50	58	14	10	12	10	67
I1	20	18	32	38	53	22	14	31	48	67	18	22	33	13	13
N2	11	10	39	23	21	9	8	19	30	32	12	5	10	3	4
S2	6	7	42	48	35	6	9	53	62	45	6	4	11	6	6
T2	10	7	16	22	24	13	11	47	29	27	8	8	18	6	6
I2	19	15	35	26	25	9	19	44	32	31	28	6	12	10	10

After correction the thickness measurements for the Spectralis™ and Cirrus™ scans were not significantly different. This may be due to the fact that the majority of the scans required minor corrections. For example, more than 50% of the Spectralis™ scans resulted in a 10 μm or less change in the central subfield thickness. Krebs *et al.* have also previously reported no significant differences in retinal thickness measurements before and after correction of segmentation errors of scans taken using Cirrus™¹¹.

The differences in the mean thickness values before and after correction in scans taken using Spectralis™ were most obvious in the central subfields of the retina (C1, N1, S1, T1, and I1) with the peripheral subfields being spared (N2, S2, T2 and I2). This may be attributed to the fact that the pathology of AMD is located centrally and therefore pathology related inaccuracies in segmentation are more likely to occur in these subfields.

Retinal thickness measurements were similar in both SD-OCT machines and were greater than Stratus™. Correction reduced the difference of the thickness measurements between the two SD-OCT devices to less than 20 μm ; in some cases as noted above, the difference was no longer statistically significant. Other studies in normal and pathologic eyes including DME and macular degeneration have also demonstrated that the difference in retinal thickness between the SD machines can be attributed to the differences in segmentation of the automated algorithms^{7,10,12}.

Despite the large numbers of scans with algorithm errors, the COR of Spectralis™ was lower for every subfield than that of Stratus™ or Cirrus™. The COR of Cirrus™ was equal to or larger than Stratus™ for both forms of the disease. In all three devices, the COR was generally better for NNV-AMD when compared to NV-AMD, especially after correction. The disease difference can be attributed to the pathology of NV-AMD disrupting the outer border, which makes it difficult for the automated algorithm to accurately segment the retinal layers^{13,14}. Krebs *et al.* evaluated the repeatability of retinal thickness measurements using Spectralis™ and Cirrus™ in patients with AMD. For images taken using Spectralis™ the mean difference between repeated measurements was found to be

within 11 μm before correction and within 1 μm after correction. For images taken using Cirrus™ the mean difference between repeated measurements was found to be within 6 μm before correction and within 4 μm after correction¹⁵. Previous studies on normal eyes have reported a high repeatability of measurements with Spectralis™, with differences between repeated measurements being within 1 μm ^{12,16}. For Stratus™ OCT images, other studies have found central subfield repeatability values in patients with NV-AMD to be 50 μm and 32–35 μm for NNV-AMD patients after correction/exclusion of scans with errors^{8,17}; our study confirms this finding. There has been one other published study looking at the repeatability of Cirrus™ OCT in NV-AMD, which found a central subfield repeatability value of 42 μm before correction and 26 μm after exclusion of scans with significant segmentation errors¹⁸. The difference between this study and our measurements may be associated with our smaller sample size. In addition, we chose not to exclude any poor quality scans, which may cause larger differences.

In addition to a lower COR, Spectralis™ also had the highest ICC values for both NV-AMD and NNV-AMD, before and after correction. For NV-AMD, Cirrus had higher coefficients after correction, and for NNV-AMD, Cirrus™ had lower coefficients as compared to Stratus™. While no previous studies have reported ICC values for AMD patients, Pierro *et al.* found comparable results in normal eyes, with Cirrus™ ICC values ranging from 83–97% and Stratus™ ICC values from 72–95%¹⁹. The most likely reason for the low repeatability and high ICC values for Spectralis™ is the eye-tracking capability, which ensures that artifacts due to eye movement are minimized and the machine scans only when the tracking software identifies the same position on the fundus¹⁶.

Bland-Altman plots indicate that there is agreement between SD-OCT machines. Correcting images also influenced agreement between machines. We found that 95% confidence intervals were narrower as compared to an SD-OCT and TD-OCT and correcting the algorithm errors further narrowed the intervals. The mean difference between machines indicates that the lowest differences were between Spectralis™ and Cirrus™, especially after correction. This is mostly likely due to the effects of manually correcting the

Table 4. 95% Confidence Intervals for Bland-Altman Plots. A: Before correction. **B:** After correction.

A. Bland-Altman 95% confidence intervals before correction (µm)									
Subfield	All eyes			NV-AMD			NNV-AMD		
	Spectralis™ vs. Cirrus™	Cirrus™ vs. Stratus™	Spectralis™ vs. Stratus™	Spectralis™ vs. Cirrus™	Cirrus™ vs. Stratus™	Spectralis™ vs. Stratus™	Spectralis™ vs. Cirrus™	Cirrus™ vs. Stratus™	Spectralis™ vs. Stratus™
Central 1 mm	42, 89	37, 65	91, 149	33, 94	43, 84	87, 166	28, 109	18, 46	63, 156
N1	29, 63	44, 65	81, 118	25, 78	44, 76	79, 136	18, 60	36, 57	67, 110
S1	21, 49	44, 71	74, 109	16, 64	44, 86	75, 131	18, 37	34, 58	58, 90
T1	21, 43	41, 59	73, 99	18, 51	37, 64	74, 109	14, 41	37, 60	58, 99
I1	23, 43	41, 74	79, 111	18, 46	28, 81	71, 115	19, 49	45, 77	72, 123
N2	13, 24	40, 61	57, 81	11, 28	37, 60	52, 87	11, 22	37, 54	50, 86
S2	16, 27	42, 73	59, 93	13, 32	42, 91	57, 118	16, 25	38, 48	55, 71
T2	9, 17	35, 49	52, 65	7, 21	29, 51	48, 69	7, 17	38, 49	52, 64
I2	9, 33	28, 51	54, 67	7, 46	15, 47	47, 64	3, 26	40, 66	58, 79
Average Width	21.5	24	30.2	35.7	35.6	45	28	20.3	38.3
B. Bland-Altman 95% confidence intervals after correction (µm)									
Subfield	All eyes			NV-AMD			NNV-AMD		
	Spectralis™ vs. Cirrus™	Cirrus™ vs. Stratus™	Spectralis™ vs. Stratus™	Spectralis™ vs. Cirrus™	Cirrus™ vs. Stratus™	Spectralis™ vs. Stratus™	Spectralis™ vs. Cirrus™	Cirrus™ vs. Stratus™	Spectralis™ vs. Stratus™
Central 1 mm	8, 30	40, 70	55, 91	5, 29	48, 91	60, 110	(-1.7-42)	18, 46	27, 75
N1	11, 34	45, 64	63, 88	13, 32	45, 74	65, 92	(-2.6, 47)	36, 57	43, 95
S1	5, 29	43, 69	56, 87	(-10, 38)	42, 83	56, 101	3, 26	34, 58	41, 78
T1	3, 21	44, 58	53, 79	46, 26	44, 62	55, 89	(-1., 22)	37, 60	35, 76
I1	4, 17	41, 74	60, 86	(-20, 19)	29, 81	55, 88	4, 22	44, 78	50, 100
N2	8, 20	39, 60	53, 74	5, 25	35, 68	46, 82	7, 16	37, 54	49, 78
S2	10, 26	41, 70	54, 90	5, 31	40, 87	50, 111	13, 23	38, 48	51, 68
T2	5, 15	34, 47	45, 60	4, 18	27, 49	44, 64	1, 15	38, 49	39, 63
I2	3, 29	29, 50	48, 60	1, 41	15, 45	42, 58	(-6, 20)	40, 66	53, 69
Average Width	18.3	22.8	25.3	25	35	36.7	23.9	20.4	34.8

Table 5. Mean difference (limits of agreement) Before Correction. A: Before correction. **B:** After correction.

Subfield	A. Mean difference (limits of agreement) before correction (µm)									
	All eyes					NV-AMD				
	Spectralis™ vs. Cirrus™	Cirrus™ vs. Spectralis™	Spectralis™ vs. Spectralis™	Spectralis™ vs. Cirrus™	Cirrus™ vs. Spectralis™	Spectralis™ vs. Spectralis™	Cirrus™ vs. Spectralis™	Spectralis™ vs. Cirrus™	Cirrus™ vs. Spectralis™	Spectralis™ vs. Spectralis™
Central 1 mm	63 (228, -101)	52 (142, -38)	120 (305, -64)	64 (220, -92)	64 (165, -37)	127 (319, -64)	69 (244, -150)	32 (85, -21)	110 (287, -68)	
N1	32 (112, -47)	50 (106, -6)	87 (168, 4)	35 (119, -49)	51 (115, -14)	92 (175, 8)	28 (85, -29)	49 (93, 7)	79 (158, 1)	
S1	34 (108, -40)	58 (142, -26)	92 (203, -20)	40 (160, -80)	65 (164, -35)	103 (235, -28)	28 (68, -13)	47 (92, 1)	75 (134, 15)	
T1	41 (143, -60)	55 (120, -10)	100 (217, -17)	52 (185, 82)	60 (138, 17)	107 (243, -27)	39 (129, -51)	47 (87, 7)	89 (172, 5)	
I1	36 (100, -29)	58 (163, -47)	96 (195, -4)	32 (103, -38)	55 (182, -72)	94 (198, -10)	34 (100, -31)	62 (123, 1)	98 (194, 2)	
N2	16 (40, -9)	42 (86, -2)	59 (98, 19)	14 (49, -19)	41 (95, -15)	59 (107, 11)	12 (34, -9)	44 (55, 23)	58 (81, 35)	
S2	25 (74, -24)	58 (154, -38)	77 (175, -21)	23 (66, -20)	67 (186, -52)	88 (214, 40)	21 (38, 4)	44 (62, 25)	63 (93, 34)	
T2	18 (50, -13)	51 (117, -15)	69 (145, -7)	20 (62, -22)	54 (132, -28)	70 (152, 13)	17 (41, -7)	46 (76, 15)	68 (138, -1)	
I2	22 (95, -50)	40 (106, -26)	54 (147, -40)	26 (116, -62)	21 (104, -42)	56 (92, 19)	15 (58, -29)	53 (99, 7)	69 (105, -33)	
Subfield	B. Mean difference (limits of agreement) after correction (µm)									
	All eyes					NV-AMD				
	Spectralis™ vs. Cirrus™	Cirrus™ vs. Spectralis™	Spectralis™ vs. Spectralis™	Spectralis™ vs. Cirrus™	Cirrus™ vs. Spectralis™	Spectralis™ vs. Spectralis™	Cirrus™ vs. Spectralis™	Spectralis™ vs. Cirrus™	Cirrus™ vs. Spectralis™	Spectralis™ vs. Spectralis™
Central 1 mm	19 (92, -54)	55 (150, -39)	73 (184, -38)	17 (80, -44)	70 (175, -34)	85 (204, 34)	20 (110, -69)	32 (85, -21)	52 (136, -33)	
N1	12 (71, -47)	52 (95, 8)	67 (145, -12)	14 (79, -52)	53 (97, 9)	73 (154, -9)	10 (60, -39)	49 (93, 7)	56 (128, -16)	
S1	17 (97, -62)	56 (139, -26)	72 (165, -21)	20 (116, -78)	62 (162, -36)	79 (185, -27)	15 (61, -31)	47 (92, 1)	60 (124, -4)	
T1	23 (97, -51)	55 (116, -6)	76 (150, 1)	23 (71, -24)	60 (131, -11)	79 (143, 15)	23 (125, -79)	47 (87, 7)	70 (161, -21)	
I1	11 (55, -33)	58 (161, -45)	73 (154, -7)	10 (59, -40)	55 (179, -68)	72 (150, -6)	13 (50, -24)	62 (123, 1)	75 (163, -12)	
N2	10 (43, -23)	41 (83, -2)	53 (99, 7)	11 (47, -24)	39 (90, -13)	54 (103, 6)	8 (37, -21)	44 (55, 23)	51 (95, 9)	
S2	19 (66, -29)	56 (148, -36)	73 (175, -30)	19 (79, -42)	64 (178, -50)	81 (210, -49)	18 (37, -1)	44 (62, 25)	60 (89, 31)	
T2	14 (53, -33)	50 (115, -16)	64 (129, -1)	16 (66, -33)	52 (132, -28)	64 (131, 3)	12 (29, -5)	46 (76, 15)	64 (129, 0)	
I2	16 (96, -64)	39 (104, -26)	54 (88, 20)	22 (115, -72)	31 (100, -39)	50 (86, 14)	7 (54, -34)	53 (99, 7)	62 (87, 37)

Figure 2a–f. Bland-Altman Plots of agreement with 95% Confidence Intervals for the 1mm central subfield. **A:** Spectralis™ vs. Cirrus™ before correction. **B:** Spectralis™ vs. Cirrus™ after correction. **C:** Cirrus™ vs. Stratus™ before correction. **D:** Cirrus™ vs. Stratus™ after correction. **E:** Spectralis™ vs. Stratus™ before correction. **F:** Spectralis™ vs. Stratus™ after correction.

Spectralis™ images and that both machines have similar scanning technologies. The limits of agreement were similarly very wide for all three machines, and were narrower after correction of images, especially for the two SD-OCT machines. Jaffe *et al.* reported similar results looking at NV-AMD, with limits of agreements being approximately 225µm between a SD-OCT and TD-OCT⁷. The poor agreement warrants caution for clinicians when trying to use the data from different machines interchangeably especially in the central 1mm of retina since most clinicians.

Our study is not without its limitations. All images were taken at a single imaging center; this might have introduced some bias. The version of software used for the Stratus™ images did not allow correction of segmentation errors and therefore these images had to be excluded from the analysis. Two independent graders manually corrected all the images; this may have resulted in some inaccuracies in segmentation line correction. In addition, in a subset of patients that had a difference in the severity of disease, both eyes were included in the analysis; this may also have resulted in possible bias. The Cirrus device that was used to capture the images did not have eye tracking and may have led to the slightly larger COR values when compared to Spectralis.

In summary, we found that although Spectralis™ had the highest frequency of errors in AMD patients, correction of images did not result in significant changes in retinal thickness due to the

errors being very small. Spectralis™ had the lowest COR values. Thus Spectralis™ maybe the best suited for examining minute morphological and thickness changes. Also, because of the wide Bland-Altman 95% intervals, there is not much agreement between the SD-OCT and TD-OCT machines. Based on our findings, we recommend that scans be carefully analyzed at reading centers before the thickness values are accepted as reliable.

Author contributions

AR and YJS and RC conceived the study. AR, MAS, RC, and EH and MS carried out the research. AR, MAS, YJS, RC and MS prepared the manuscript. YJS and MAS provided statistical support. DVD and QDN supervised the project. All authors were involved in the revision of the draft manuscript and have agreed to the final content.

Competing interests

No competing interests were disclosed.

Grant information

The author(s) declared that no grants were involved in supporting this work.

Acknowledgments

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Appendix A

The following ETDRS grid depicts the abbreviations for the nine subfields. C1 – Central 1mm. N1 – Inner nasal. S1 – Inner superior. T1 – Inner temporal. I1 – Inner inferior. N2 – Outer nasal. S2 – Outer superior. T2 – Outer temporal. I2 – Outer inferior.

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Akshay Nair

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This study was performed to assess the reproducibility and reliability of optical coherence tomography scans obtained using the time domain (TD-OCT) Stratus OCT, and the Spectral Domain (SD-OCT) Spectralis and Cirrus OCT devices before and after manual correction.

The title and abstract are appropriate. The possible errors and drawbacks have been addressed and mentioned in the manuscript. The statistical analysis is appropriate and the authors have presented acceptable conclusions. The conclusions are acceptable and balanced; however, the number of eyes included in the study could have been more. The previous reviewers have addressed important point which have been duly taken into consideration by the authors.

Competing Interests: No competing interests were disclosed.

I confirm that I have read this submission and believe that I have an appropriate level of expertise to confirm that it is of an acceptable scientific standard.

Reviewer Report 17 March 2015

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Igor Kozak

Vitreoretinal Division, King Khaled Eye Specialist Hospital, Riyadh, Saudi Arabia

The authors have addressed all reviewers comments.

Competing Interests: No competing interests were disclosed.

I confirm that I have read this submission and believe that I have an appropriate level of expertise to confirm that it is of an acceptable scientific standard.

Version 1

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Igor Kozak

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This study reports on reliability and reproducibility of optical coherence tomography (OCT) scans before and after manual correction in eyes with age-related macular degeneration (AMD). It concludes that manual correction improves automated segmentation and that the agreement, as evidenced by intraclass correlation coefficients and coefficients of repeatability, is better between spectral-domain OCT instruments. The study brings important numerical comparisons of measurements of central foveal thickness using different instruments. Such comparisons are crucial especially with transitioning from time-domain to spectral-domain OCT technology in ongoing and future clinical trials. The paper is well written. Minor comments for authors:

1. The same operator acquired OCT scans of the same eyes on the same instruments. It would be useful to know how many graders and how independently performed manual correction at the Reading Center.
2. The Spectralis system via TruTrack provides excellent ability to perform follow-up scans from the exact retinal areas. How was this dealt with using other two systems in order to avoid sampling error?
3. Misidentification of inner retinal layer is a common artifact and has been found in a large number of scans including the instruments used in this study. The authors are encouraged to cite some of those studies such as [Ho et al. \(2009\)](#).
4. Another useful study to mention with respect to comparing time-domain and spectral-domain OCT instruments: [Mylonas et al. \(2009\)](#).
5. Based on a study of reproducibility in Stratus OCT, any artifact resulting in an error that is more than 50µm is clinically significant, suggesting 50 µm as a cutoff for retreatment of neovascular AMD patients ([Patel et al., 2009](#)). In another study any artifacts resulting in automated segmentation errors of more than 10% of the actual (manually measured) ETDRS center subfield thickness were considered clinically significant ([Browning et al., 2008](#)).

In this study, some of the variations after manual correction surpassed these margins. Maybe some comment in Discussion regarding this issue.

Competing Interests: No competing interests were disclosed.

I confirm that I have read this submission and believe that I have an appropriate level of expertise to confirm that it is of an acceptable scientific standard.

Reviewer Report 03 February 2014

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Ilse Krebs

Department of Ophthalmology, Rudolf Foundation Clinic, Vienna, Austria

The reproducibility of retinal thickness measurements with different OCT devices in eyes with age-related macular degeneration before and after error correction is presented. This is a topic of high interest and actuality. The title and Abstract are appropriate.

- *"To date, no other study has examined the effects of manual correction of the thickness algorithm in SD-OCT and TD-OCT machines in eyes with AMD."*
- *"At this point, we are not aware of any previous study looking at the repeatability of Spectralis™ images in AMD."*

This is not really true, and I want to refer to publications dealing with this topic (Krebs *et al.* 2012; Krebs *et al.*, 2011; Krebs *et al.*, 2009). The results of these studies should be discussed, as some of the results are confirmed by the results of the current study. Most of the studies focus only on the central 1000µm area, whereas in this study also more peripheral areas were examined. This should be discussed a little bit more because this might be interesting: were the failures only in the central part, or also in the periphery (the pathology of neovascular AMD is located centrally therefore pathology related failures should occur only in the central area.)

- It is mentioned in the discussion section, but it should also added to the methods: how many observers assessed the segmentation errors, and performed the error correction?
- The lack of significant differences before and after correction might be due to the small number of examinations requiring correction.
- The sample size seems to be quite low, was there any calculation when planning this study? A possible bias of including both eyes in a part of patients should be mentioned.

Competing Interests: No competing interests were disclosed.

I confirm that I have read this submission and believe that I have an appropriate level of

expertise to confirm that it is of an acceptable scientific standard, however I have significant reservations, as outlined above.

Author Response () 28 Feb 2014

Yasir Sepah, Stanford University, USA

Dear Dr. Krebs,

Thank you for your valuable comments. We agree that our study is not the only study that has tried to deal with this topic. We will make changes to the manuscript to clarify this statement.

We will add the results and analysis of the peripheral areas to the discussion in the revision.

No sample size calculation was performed before the conduct of the study. Two eyes of the same patient were included because of difference in the severity of the disease between the two eyes of the same patient. The control group patients contributed only one eye to the analysis.

Competing Interests: None

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